



Equations and Calculations

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Introduction

The human body is a complex, interconnected system where physiological processes are meticulously regulated to maintain homeostasis. Among the most critical of these processes are the respiratory, cardiac functions, and the acid-base balance, each of which plays a vital role in sustaining life. Understanding the underlying principles of these systems requires not only a grasp of their anatomy and physiology but also a familiarity with the mathematical equations that quantify their functions. These equations serve as foundational tools for clinicians, researchers, and students, providing a framework to analyze, diagnose, and treat a wide range of physiological and pathological conditions.

This chapter delves into the key equations governing these systems, exploring their derivation, application, and significance in both physiological and pathological contexts. By mastering these concepts, we gain a deeper appreciation of the intricate mechanisms that sustain life and the tools to intervene when these mechanisms falter.

Respiratory & Cardiovascular Equations

Alveolar Oxygen Gas Equation (PAO₂)

Used to estimate the partial pressure of oxygen in the alveoli (Normal: 104 mmHg at sea level)

$$PAO_2 = FIO_2 (P_{atm} - P_{H_2O}) - PACO_2 / R$$

- FIO₂: Fraction of inspired oxygen (e.g. 0.21 for room air).
 - P_{atm}: Atmospheric pressure (760 mmHg at sea level).
 - P_{H₂O}: Partial pressure of water vapor (47 mmHg at body temperature).
 - PACO₂: Alveolar partial pressure of carbon dioxide (assumed equal to arterial PaCO₂).
 - R: Respiratory exchange ratio (typically 0.8).
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Alveolar Carbon Dioxide Equation (PACO₂)

Describes the relationship between alveolar ventilation and alveolar partial pressure of CO₂ (Normal 40 mmHg)

$$PACO_2 = VCO_2 / VA \times 0.863$$

- VA: Alveolar ventilation
 - VCO₂ : CO₂ production
 - 0.863: Constant K
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Alveolar-Arterial Oxygen Gradient (A-a)

Evaluates gas exchange efficiency (Normal: 10 - 20)

$$A-a \text{ Gradient} = PAO_2 - PaO_2$$

- PAO₂: Alveolar oxygen partial pressure (from Alveolar Gas Equation).
 - PaO₂: Arterial oxygen partial pressure.
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Partial Pressure of Inspired Oxygen (PIO₂)

The oxygen pressure in inspired air (Normal: 90 – 100 mmHg)

$$PIO_2 = FIO_2 \times (P_{atm} - P_{H_2O})$$

- PIO₂: Inspired oxygen partial pressure (mmHg).
 - FIO₂: Fraction of inspired oxygen.
 - P_{atm}: Atmospheric pressure (760 mmHg at sea level).
 - P_{H₂O}: Water vapor pressure (47 mmHg at 37°C).
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Arterial Oxygen Content (CaO₂)

Determines the total oxygen content (CaO₂) in arterial blood (Normal: 16 – 20 mL O₂/dL)

$$CaO_2 = (1.34 \times Hb \times SpO_2) + (0.0034 \times PaO_2)$$

- Hb: Hemoglobin concentration (g/dL).
 - SpO₂: Oxygen saturation of hemoglobin (as a fraction, e.g. 0.97 for 97%).
 - PaO₂: Partial pressure of oxygen in arterial blood (mmHg).
 - 1.34: Oxygen carrying capacity of hemoglobin (mL O₂ per g of Hb).
 - 0.003: Solubility of oxygen in plasma (mL O₂ per mmHg per dL).
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Venous Oxygen Content (CvO₂)

This calculates the oxygen content in venous blood, analogous to arterial oxygen content but using mixed venous parameters (Normal: 12 – 16 mL O₂/dL)

$$CvO_2 = (1.34 \times Hb \times SvO_2) + (0.0034 \times PvO_2)$$

- Hb: Hemoglobin concentration (g/dL).
 - SvO₂: Oxygen saturation of hemoglobin (as a fraction, e.g., 0.75 for 75%).
 - PvO₂: Partial pressure of oxygen in mixed venous blood (mmHg).
 - 1.34: Oxygen carrying capacity of hemoglobin (mL O₂ per g of Hb).
 - 0.003: Solubility of oxygen in plasma (mL O₂ per mmHg per dL).
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Fick's Principle

Used to calculate oxygen consumption (VO_2):

$$\text{VO}_2 = Q \times (\text{CaO}_2 - \text{CvO}_2)$$

- Q: Cardiac output (L/min).
- CaO_2 : Arterial Oxygen Content (mLO₂/dL)
- CvO_2 : Venous Oxygen Content (mLO₂/dL)

The equation can be rearranged as:

$$Q = \text{VO}_2 / (\text{CaO}_2 - \text{CvO}_2)$$

Oxygen Delivery (DO_2)

This calculates the total amount of oxygen delivered to tissues per minute (Normal: 900 - 1100 mL O₂/min)

$$\text{DO}_2 = Q \times \text{CaO}_2$$

- DO_2 : Oxygen delivery (mL O₂/min).
 - Q: Cardiac output (L/min, converted to mL/min by multiplying by 1000).
 - CaO_2 : Arterial oxygen content (mLO₂/dL)
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Oxygen Uptake (VO_2)

Measures oxygen uptake by tissues (Normal: 250-300 mL O₂/min)

$$\text{VO}_2 = \text{VE} \times (\text{FIO}_2 - \text{FEO}_2)$$

- VO_2 = Oxygen uptake (mLO₂/min).
 - VE = Minute ventilation (L/min).
 - FIO_2 = Fraction of inspired oxygen (e.g. 0.21 for room air).
 - FEO_2 = Fraction of expired oxygen (typically 0.16 - 0.17 in normal breathing).
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Oxygen Extraction Ratio (OER)

This measures the proportion of oxygen that is extracted by tissues (Normal: 22-30%)

$$\text{OER} = \text{CaO}_2 - \text{CvO}_2 / \text{CaO}_2$$

- CaO_2 : Arterial oxygen content.
- CvO_2 : Venous oxygen content.

Alternatively, OER can be expressed using oxygen saturations directly:

$$\text{OER} = \text{SaO}_2 - \text{SvO}_2 / \text{SaO}_2$$

Carbon Dioxide Output (VCO_2)

Measures the amount of CO_2 produced and exhaled per minute (Normal: 2-3 $\text{mLCO}_2/\text{kg}/\text{min}$)

$$\text{VCO}_2 = \text{VE} \times (\text{FECO}_2 - \text{FICO}_2)$$

- VCO_2 = Carbon dioxide output ($\text{mL CO}_2/\text{min}$).
 - VE = Minute ventilation (L/min).
 - FECO_2 = Fraction of expired CO_2 (typically 0.04 or 4% in normal breathing).
 - FICO_2 = Fraction of inspired CO_2 (~ 0 , since inhaled CO_2 is negligible in room air).
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Shunt Fraction (Qs/Qt)

Estimates the fraction of blood bypassing ventilated alveoli, often used in hypoxemia (Normal $< 5\%$)

$$\text{Qs} / \text{Qt} = \text{CcO}_2 - \text{CaO}_2 / \text{CcO}_2 - \text{CvO}_2$$

- Qs/Qt : Shunt fraction (unitless).
 - CcO_2 : Oxygen content in capillary blood (mLO_2/dL).
 - CaO_2 : Arterial oxygen content (mLO_2/dL).
 - CvO_2 : Venous oxygen content (mLO_2/dL).
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Respiratory Quotient (RQ)

Describes the ratio of carbon dioxide production to oxygen consumption (Normal: 0.8)

$$RQ = VCO_2 / VO_2$$

- RQ: Respiratory quotient (unitless).
 - VCO_2 : Rate of carbon dioxide production (mL/min).
 - VO_2 : Rate of oxygen consumption (mL/min).
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Ventilation-Perfusion Ratio (V/Q)

Describes the relationship between alveolar ventilation and pulmonary blood flow (Normal: 0.8)

$$V/Q = VA / Q$$

- VA = Alveolar ventilation (L/min).
 - Q = Pulmonary blood flow (L/min), equivalent to cardiac output (Q)
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Minute Ventilation (VE)

Total volume of air moved in and out of the lungs per minute (Normal: 5 – 8 L/min)

$$VE = VT \times RR$$

- VT : Tidal volume (L).
 - RR : Respiratory rate (breaths per minute).
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Alveolar Ventilation (VA)

Volume of air reaching the alveoli per minute, excluding dead space (Normal 4 – 5 L/min)

$$VA = (VT - VD) \times RR$$

- VT: Tidal volume (L).
 - VD: Dead space volume (L).
 - RR: Respiratory rate (breaths per minute).
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Alveolar Ventilation Equation

Measures efficiency of ventilation (Normal 4 – 5 L/min)

$$VA = VCO_2 \times k / PACO_2$$

- VA = Alveolar ventilation (L/min).
 - VCO₂ = CO₂ production (mL/min).
 - PACO₂ = Alveolar CO₂ partial pressure (mmHg).
 - k = 0.863 (Constant)
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Dead Space (VD) Bohr Equation

Estimates physiological dead space (Normal 20 - 35%)

$$VD/VT = PaCO_2 - PECO_2$$

- PaCO₂: Arterial partial pressure of CO₂.
 - PECO₂: Mixed expired partial pressure of CO₂.
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Dead Space Volume (VD) Fowler's Equation

Measures anatomical dead space (Normal: 2.2 ml/kg IBW)

$$VD = VT \times \frac{PaCO_2 - PECO_2}{PaCO_2}$$

- VT: Tidal volume.
 - PaCO₂: Arterial partial pressure of CO₂.
 - PECO₂: Expired CO₂ partial pressure.
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Capnography Equation (End-Tidal CO₂)

Measures CO₂ pressure in exhaled breath (Normal 30 – 40 mmHg)

$$ETCO_2 = PaCO_2 - (VD / VT \times PaCO_2)$$

- ETCO₂ = End-tidal CO₂.
 - VD/VT = Dead space fraction.
 - PaCO₂ = Arterial CO₂.
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Airway Resistance (RAW)

Quantifies resistance to airflow in the respiratory system (Normal: 0.5 – 2.5 cmH₂O/L/sec)

$$Raw = \Delta P / \dot{V}$$

- Raw: Airway resistance (cmH₂O/L/sec).
 - ΔP: Pressure difference across the airway (cmH₂O).
 - \dot{V} : Airflow (L/sec).
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Respiratory System Compliance (CRS)

Describes the distensibility of the lungs and chest wall (Normal: 70 – 100 mL/cmH₂O)

$$C = \Delta V / \Delta PC$$

- C: Compliance (mL/cmH₂O).
 - ΔV (Delta V): Change in volume (mL).
 - ΔP (Delta P): Change in airway pressure (cmH₂O).
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Chest Wall Compliance (CCW)

Describes the distensibility of the lungs and chest wall (Normal: 150 - 200 mL/cmH₂O)

$$C = \Delta V / \Delta PC$$

- C: Compliance (mL/cmH₂O).
 - ΔV (Delta V): Change in volume (mL).
 - ΔP (Delta P): Change in pleural (esophageal) pressure (cmH₂O).
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Lung Compliance (CL)

Describes the distensibility of the lungs and chest wall (Normal: 150 - 200 mL/cmH₂O)

$$C = \Delta V / \Delta PC$$

- C: Compliance (mL/cmH₂O).
 - ΔV (Delta V): Change in volume (mL).
 - ΔP (Delta P): Change in trans-pulmonary pressure (cmH₂O).
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Time Constant (τ)

Time required for inflation or deflation up to 63% of the final volume (Normal 0.8 – 1.2 seconds)

$$\tau = \text{CRS} \times \text{RAW}$$

- τ = Time constant (seconds).
 - CRS = Respiratory system compliance (L/cmH₂O).
 - RAW = Airway resistance (cmH₂O/L/s).
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Diffusing Capacity (DLCO)

Represents the lung's ability to transfer gas (Normal 75% - 140% of predicted value)

$$\text{DLCO} = \dot{V}\text{CO} / \Delta\text{PCO}$$

- $\dot{V}\text{CO}$: Uptake of carbon monoxide (mL/min).
 - ΔPCO : Partial pressure difference of carbon monoxide across the alveolar-capillary membrane.
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Peak Expiratory Flow Rate (PEFR)

A clinical measure of airway obstruction (Normal: 400 – 700 L/min)

$$\text{PEFR} = \Delta V / \Delta t$$

- PEFR: Peak Expiratory Flow rate (L/min)
 - ΔV : Volume of air exhaled.
 - Δt : Time taken to exhale that volume.
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Oxygen-Hemoglobin Dissociation Equation

Estimates oxygen binding to hemoglobin:

$$SO_2 / 1 - SO_2 = 10^{(PO_2 - P50) / n}$$

- SO_2 : Oxygen saturation.
 - PO_2 : Partial pressure of oxygen.
 - $P50$: PO_2 at 50% saturation (typically ~26.6 mmHg).
 - n : Hill coefficient (~2.7 for hemoglobin).
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Pulmonary Vascular Resistance (PVR)

Calculates resistance in the pulmonary circulation (Normal: 30 - 180 dyn/s/cm⁻⁵)

$$PVR = PPA - PLA / Q$$

- PVR: Pulmonary vascular resistance (dyn·s·cm⁻⁵).
 - PPA: Mean pulmonary artery pressure (mmHg).
 - PLA: Left atrial pressure or pulmonary capillary wedge pressure (mmHg).
 - Q: Cardiac output (L/min).
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Systemic Vascular Resistance (SVR)

Calculates resistance in the systemic circulation (Normal: 800 and 1200 dynes·sec/cm⁻⁵)

$$SVR = PSA - PRA / Q$$

- SVR: Systemic vascular resistance (dyn·s·cm⁻⁵).
 - PSA: Mean systemic artery pressure (mmHg).
 - PRA: Right atrial pressure or central venous pressure (mmHg).
 - Q: Cardiac output (L/min).
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Acid – Base Equations

Henderson-Hasselbalch Equation

Explains the relationship of HCO_3 and PaCO_2 to maintain pH

$$\text{pH} = \text{pKa} + \log \left(\frac{[\text{HCO}_3]}{0.03 \times \text{PaCO}_2} \right)$$

- pKa: 6.1 (for bicarbonate buffer system).
 - $[\text{HCO}_3]$: Bicarbonate concentration (mEq/L).
 - PaCO_2 : Arterial CO_2 pressure (mmHg).
 - 0.03 = Solubility constant of CO_2 in plasma.
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Respiratory Compensation for Metabolic Disorders

Metabolic Acidosis (Winter's formula):

$$\text{PaCO}_2 = (1.5 \times \text{HCO}_3) + 8 \pm 2$$

Predicts expected PaCO_2 in metabolic acidosis

If actual $\text{PaCO}_2 >$ expected, there is a concurrent respiratory acidosis, if $<$ there is concurrent respiratory alkalosis.

For Metabolic Alkalosis:

$$\text{PaCO}_2 = (0.7 \times \text{HCO}_3) + 20 \pm 5$$

Predicts expected PaCO_2 in metabolic alkalosis.

If PaCO_2 is $<$ than expected, there is concurrent respiratory alkalosis, if $>$ there is concomitant respiratory acidosis.

Metabolic Compensation for Respiratory Disorders

Acute Respiratory Acidosis (\uparrow PaCO₂):

$$\Delta\text{HCO}_3 = \Delta\text{PaCO}_2 / 10 \times 1$$

For every 10 mmHg \uparrow in PaCO₂, HCO₃ increases by 1 mEq/L (hours).

Chronic Respiratory Acidosis (\uparrow PaCO₂):

$$\Delta\text{HCO}_3 = \Delta\text{PaCO}_2 / 10 \times 3-4$$

For every 10 mmHg \uparrow in PaCO₂, HCO₃ increases by 3-4 mEq/L (days).

Acute Respiratory Alkalosis (\downarrow PaCO₂):

$$\Delta\text{HCO}_3 = \Delta\text{PaCO}_2 / 10 \times 2$$

For every 10 mmHg \downarrow in PaCO₂, HCO₃ decreases by 2 mEq/L (hours).

Chronic Respiratory Alkalosis (\downarrow PaCO₂):

$$\Delta\text{HCO}_3 = \Delta\text{PaCO}_2 / 10 \times 4-5$$

For every 10 mmHg \downarrow in PaCO₂, HCO₃ decreases by 4-5 mEq/L (days).

Disorder	Primary Change	Compensation	Expected Compensation
Respiratory Acidosis	$\uparrow\text{PCO}_2$	Kidneys retain HCO_3^- excrete H^+	Acute: $\Delta\text{HCO}_3^- = +1 \text{ mEq/L per } 10 \text{ mmHg } \Delta\text{PCO}_2$ Chronic: $\Delta\text{HCO}_3^- = +3.5 \text{ mEq/L per } 10 \text{ mmHg } \Delta\text{PCO}_2$
Respiratory Alkalosis	$\downarrow\text{PCO}_2$	Kidneys excrete HCO_3^- retain H^+	Acute: $\Delta\text{HCO}_3^- = -2 \text{ mEq/L per } 10 \text{ mmHg } \Delta\text{PCO}_2$ Chronic: $\Delta\text{HCO}_3^- = -4-5 \text{ mEq/L per } 10 \text{ mmHg } \Delta\text{PCO}_2$
Metabolic Acidosis	$\downarrow\text{HCO}_3^-$	Lungs hyperventilate to $\downarrow\text{PCO}_2$	$\text{PCO}_2 = (1.5 \times \text{HCO}_3^-) + 8 \pm 2$ (Winter's Formula)
Metabolic Alkalosis	$\uparrow\text{HCO}_3^-$	Lungs hypoventilate to $\uparrow\text{PCO}_2$	$\Delta\text{PCO}_2 = +0.7 \text{ mmHg per } 1 \text{ mEq/L } \Delta\text{HCO}_3^-$

Table 1: Summary of Compensation Mechanisms.

Anion Gap (AG) Calculation for Metabolic Acidosis

$$AG = Na - (Cl + HCO_3)$$

- Na^+ = Serum sodium (normal: 135–145 mEq/L).
- Cl^- = Serum chloride (normal: 96–106 mEq/L).
- HCO_3^- = Serum bicarbonate (normal: 22–26 mEq/L).
- Normal Anion Gap = 8–12 mEq/L.

Increased AG (>12 mEq/L) = High Anion Gap Metabolic Acidosis

Normal AG (8–12 mEq/L) = Non-Anion Gap Metabolic Acidosis

Corrected Anion Gap for Albumin

$$AG \text{ corrected} = AG + 2.5 \times (4 - \text{Albumin})$$

Delta-Delta Equation (For Mixed Acid-Base Disorders)

$$\Delta AG / \Delta HCO_3$$

- $\Delta AG = (\text{Measured AG} - \text{Normal AG})$.
- $\Delta HCO_3 = (\text{Normal } HCO_3 - \text{Measured } HCO_3)$.

If $\Delta AG / \Delta HCO_3 \approx 1$ Pure AG metabolic acidosis.

> 1 Concurrent metabolic alkalosis.

< 1 Concurrent normal AG metabolic acidosis.

Strong Ion Difference (SID)

Stewart's Acid-Base Approach to assess metabolic acidosis/alkalosis. (Normal 40 – 50 mEq/L)

$$\text{SID} = (\text{Na} + \text{K} + \text{Ca} + \text{Mg}) - (\text{Cl} + \text{other anions})$$

- SID: Strong ion difference (mEq/L).
 - Na: Serum Sodium (135 – 145 mEq/L).
 - K: Serum Potassium (3.5 – 5 mEq/L).
 - Ca: Serum Calcium (4.4 – 5.2 mEq/L) (8.8 – 10.4 mg/dL).
 - Mg: Serum Magnesium (1.3 – 2.1 mEq/L).
 - Cl: Serum Chloride (95 – 105 mEq/L).
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Base Excess (BE)

$$\text{BE} = 0.93 \times (\text{HCO}_3 - 24.4) + 14.83 \times (\text{pH} - 7.4)$$

- BE: Base Excess.
- HCO_3 : serum Bicarbonate.
- 0.93: Constant for the buffering capacity of HCO_3 .
- 14.83: Constant for the buffering capacity of hemoglobin and other plasma proteins.

Determines how much base/acid is needed to return pH to normal.

BE > 2 = Metabolic alkalosis, BE < -2 = Metabolic acidosis.

Laws of Physics

Boyle's Law (Pressure-Volume Relationship)

$$P_1 V_1 = P_2 V_2$$

- P: Pressure.
- V: Volume.

Boyle's Law, in the context of the lungs, describes the inverse relationship between the volume of the lungs and the pressure within them.

Dalton's Law of Partial Pressures

$$P_{\text{gas}} = F_{\text{gas}} \times P_{\text{total}}$$

- P_{gas} : Partial pressure of a gas.
- F_{gas} : Fraction of the gas in the mixture.
- P_{total} : Total atmospheric pressure.

Dalton's Law states that the total pressure of the air is the sum of the partial pressures of each of these gases. Each gas contributes to the overall atmospheric pressure in proportion to its concentration in the air.

Henry's Law (Gas Dissolution in Blood)

$$C = kP$$

- C: Concentration of dissolved gas.
- K: Henry's constant.
- P: Partial pressure of gas.

Henry's Law states that the amount of a gas that dissolves in a liquid is directly proportional to the partial pressure of that gas above the liquid, provided the temperature remains constant.

Fick's First Law of Diffusion

$$V = AD (P_1 - P_2) / T$$

- V: Gas diffusion rate.
- A: Surface area.
- D: Diffusion coefficient.
- $P_1 - P_2$: Pressure difference.
- T: Thickness of the membrane.

Fick's First Law of Diffusion states that the rate of diffusion of a substance is proportional to the concentration gradient and the area available for diffusion.

Poiseuille's Law

$$Q = (\pi \Delta P r^4) / (8 \eta l)$$

- Q: Flow rate
- ΔP : Pressure difference
- R: Radius of the tube
- H: Viscosity of the fluid
- L: Length of the tube

Poiseuille's Law explains the factors affecting airway resistance in regulating airflow in the lungs.

Laplace's Law

$$T = Pr$$

- T: Wall tension
- P: Pressure
- r: Radius of the cylinder

Laplace's Law states that the tension in the wall of a sphere is proportional to the product of the pressure inside the sphere or cylinder and the radius of the sphere

Ideal Gas Law

$$PV = nRT$$

- P: Pressure
- V: Volume
- N: Number of moles of gas
- R: Ideal gas constant
- T: Temperature (in Kelvin)

The Ideal Gas Law explains how changes in volume, temperature, and pressure are related to each other.

Bernoulli's Principle

$$P + \frac{1}{2} \rho v^2 + \rho gh = \text{constant}$$

- P: Pressure
- ρ : Density of the fluid
- V: Velocity of the fluid
- g: Acceleration due to gravity
- h: Height

Bernoulli's principle explains the relationship between the pressures, density and velocity of fluids or gas.

Hooke's Law

$$F = -kx$$

- F: Force
- K: Spring constant (lung stiffness)
- x: Displacement from equilibrium (change in volume)

Hooke's Law describes the elastic behavior of the lungs, the balance between the forces that expand the lungs (muscle contraction) and the elastic recoil forces determines the volume of air that moves in and out of the lungs.

Conclusion

The study of respiratory, cardiac, and acid-base equations is not merely an academic exercise but a fundamental aspect of understanding human physiology and pathology. These equations provide a quantitative lens through which we can analyze the intricate interplay between the respiratory, cardiovascular, and metabolic systems, each of which is essential for maintaining homeostasis. From assessing oxygen delivery and carbon dioxide elimination to evaluating cardiac performance and acid-base balance, these mathematical tools empower clinicians and researchers to diagnose, monitor, and treat a wide array of conditions with precision and insight.

As we continue to advance our understanding of human health and disease, the principles and equations discussed in this chapter remain indispensable. They not only deepen our comprehension of normal physiological processes but also provide a foundation for identifying and addressing pathological deviations. By integrating these concepts into clinical reasoning, we are better equipped to improve patient outcomes and advance the field of medicine. Ultimately, mastering these equations is a step toward unraveling the complexities of the human body and harnessing that knowledge to promote health and healing.

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